Determining TG-43 brachytherapy dosimetry parameters and dose distribution for a ¹³¹Cs source model CS-1

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Background: Monte Carlo determination of TG-43 brachytherapy dosimetry parameters and dose distribution calculation for 131Cs source model CS-1 are presented in this study. Materials and Methods: The dose distribution was calculated around the 131Cs Model CS-1 located in the center of 30 cm ×30 cm ×30 cm water, and soft tissue phantoms cube using MCNP code by Monte Carlo method. The percentage depth dose (PDD) variation along the different axis. parallel and perpendicular, the source was calculated. Then, the isodose curves for 100%, 75%, 50% and 25% PDD were constructed. Finally, $F(r,\theta)$ and g(r)dosimetry parameters of TG-43 protocol have been determined. Results: Results obtained show that the Monte Carlo method could only calculate dose deposition in high gradient region, near the source, accurately. The energy cut off was found to be 1 eV and the error in the calculations was less than 2%. Conclusion: The isodose curves of the CS-1 131Cs source were constructed from dose calculation by MCNP code. The calculated dosimetry parameters for the source were in agreement with previously published results. Iran. J. Radiat. Res., 2007; 5 (2): 85-90

Keywords: ¹³¹Cs source, dose distribution, isodose curves, MCNP code.

INTRODUCTION

Theoretical and experimental dosimetric have been supplied information on the dependence of the brachytherapy geometry source materials (1-5). Usually, Monte Carlo method is used to define dose distribution function, the radial dose variation, and the dose calculation close to the source brachytherapy. Chen et al. (6). calculated the distribution of absorbed dose around commercially available 131Cs seeds model Cs-1 by Monte Carlo simulation.

¹³¹Cs has a higher average energy than any other commonly used prostate brachytherapy isotope in the market such as ¹⁰³Pd and ¹²⁵I. Energy is a key factor in how uniformly the radiation dose can be delivered throughout

the prostate. Also, ¹³¹Cs has the shortest halflife of any prostate brachytherapy isotope at 9.7 days. ¹³¹Cs delivers 90% of the prescribed dose to the prostate in just 33 days compared to 58 days for 103Pd and 204 days for 125I. The short half-life of 131Cs reduces the duration of time during which the prostate receives the irritating effects of the radiation. Another benefit to the short half-life of ¹³¹Cs is what is known as the biological effective dose (BED). BED is a way for providers to predict how an isotope will perform against slow versus fast growing tumors. Studies have shown ¹³¹Cs is able to deliver a higher BED across a wide range of tumor types than either 125I or 103Pd. Although prostate cancer is typically viewed as a slow growing cancer it can present with aggressive features. 131Cs's higher BED may be particularly beneficial in such situations. Currently, the IsoRay ¹³¹Cs seed is used exclusively for the treatment of prostate cancer (7-12). For calculating dose distribution TG-43 brachytherapy parameters usually Monte Carlo codes as MCNP, EGS4, GEANT4 are applied. In this present work, we have used MCNP4C code (12) to calculate relative dose in the phantom.

MATERIALS AND METHODS

¹³¹Cs source

The $^{131}\mathrm{Cs}$ seed was developed after invention by Lawrence and a $^{131}\mathrm{Cs}$ (model Cs-1) received 510(k) FDA clearance in 2003 $^{(11)}$. New low-energy interstitial brachytherapy seeds containing $^{131}\mathrm{Cs}$ source model Cs-1 were

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Fax: +98 571 4411161 E-mail: amowlavi@sttu.ac.ir introduced by IsoRay Medical Inc. The ¹³¹Cs with a half life of 9.7 days emits γ-ray with highest peaks from 29 to 34 keV (3). Offsetting, with the disadvantage of its high specific activity, translated into possibility of developing physically small, high-activity sources as a replacement for ¹⁹²Ir in brachytherapy (10)</sup>.

Figure 1 shows a schematic cross-sectional view of the IsoRay ¹³¹Cs brachytherapy seed (Model CS-1). The titanium tube has an outer diameter of 0.8 mm with a wall thickness of 0.05 mm, thus an inner diameter of 0.7 mm. The center X-ray marker is a 0.25 mm diameter gold wire. The wire is surrounded by a glass and ceramic tube with nominal dimensions of 0.4 mm inside diameter and 0.65 mm outside diameter. The overall lengths of the seeds tested were 4.7 mm, based on a 4.5-mm long tube with 0.1 mm thick caps on each end. The core length was 4.2 mm to allow clearance inside the tube for fit-up and welding (2, 3). We assumed the radioactive material to be uniformly distributed within the ¹³¹Cs active core. The photons spectrum emitted per decay of 131Cs and their intensity are shown in table 1 ...

Method of dose calculation in water and soft tissue phantoms

The Monte Carlo N-Particle code (MCNP) version 4C) with photon cross-section library DLC-200 was used for the dose rate simulations (12). The cutoff energy was set at 1.0 keV. In the present work, the dose distribution has been calculated around the ¹³¹Cs source, located in the center of 30cm ×30cm ×30 cm phantom as shown in figure 2 by using tally F6:p of MCNP code (12). The tally in the sphere of 0.1 mm diameter cell was evaluated as dose in the point center of

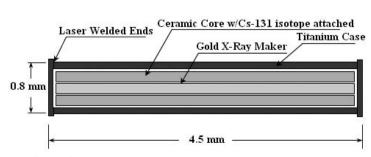


Figure 1. Schematic diagram of the CS-1 131Cs source structure

Table 1. The photon spectrum of 131Cs source is used in our simulation.

Energy (keV)	Radiation Source	Intensity
16.6	Fluorescenct (Nb - K_{α})	0.007 ± 0.0003
18.7	Fluorescenct (Nb - K_{β})	0.001 ± 0.00006
29.7	$^{131}\mathrm{Cs}$ - K_{lpha}	1.000
33.6	$^{131}\mathrm{Cs}$ - $\mathrm{K}_{\beta1,\;\beta3}$	0.201 ± 0.0007
34.4	$^{131}\mathrm{Cs}$ - $\mathrm{K}_{\beta2}$	0.050 ± 0.0003

the sphere. First, along the X axis with 0.1 mm step and along the Y axis with 0.1 mm step, and the relative dose curves were calculated. The dose distribution was normalized to 100% at the point X=2 mm, Y=0 mm, arbitrary. Isodose points were found from relative dose curves by interpolate method. Soft tissue composition used in this study, are listed in table 2 (15). Mass density for soft tissue was 1.04 g/cm³.

TG-43 formalism

Radial dose function and anisotropy function are dosimetry important parameters that must be determined according to TG-43 protocol, further to the comparison of our result with those obtained by others. According to the published protocol $D(r,\theta)$ the absorbed dose rate, $F(r,\theta)$ is the anisotropy function, g(r) is radial dose function are expressed as:

$$\dot{\mathbf{D}}(\mathbf{r}, \boldsymbol{\theta}) = \mathbf{S}_{k} \Lambda \frac{\mathbf{G}(\mathbf{r}, \boldsymbol{\theta})}{\mathbf{G}(\mathbf{r}_{0}, \boldsymbol{\theta}_{0})} \mathbf{g}(\mathbf{r}) \mathbf{F}(\mathbf{r}, \boldsymbol{\theta}) \tag{1}$$

$$\dot{D}(r,\theta) = S_k \Lambda \frac{G(r,\theta)}{G(r_0,\theta_0)} g(r) F(r,\theta)$$

$$F(r,\theta) = \frac{\dot{D}(r,\theta)}{\dot{D}(r,\theta_0)} \frac{G(r,\theta_0)}{G(r,\theta)}$$
(2)

$$g(r) = \frac{\dot{D}(r, \theta_0)}{\dot{D}(r_0, \theta_0)} \frac{G(r_0, \theta_0)}{G(r, \theta_0)}$$
(3)

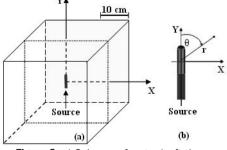


Figure 2. a) Scheme of water/soft tissue phantom which 131Cs source id located in the centre of cube, b) the source in large size.

Table 2. Soft tissue composition and mass density for soft tissue used in MCNP input (15).

Element	Weight Fraction	Element	Weight Fraction
Н	10.454	S	0.204
\mathbf{C}	22.663	Cl	0.133
N	2.490	K	0.208
O	63.525	Ca	0.024
Na	0.112	Fe	0.005
Mg	0.013	Zn	0.003
SiO	0.030	Rb	0.001
P	0.134	Zr	0.001

Where S_k is the air kerma strength, Λ is the dose rate constant, $G(r,\theta)$ is the geometry factor, and (r_0,θ_0) is the reference point.

RESULTS

Monte Carlo dose calculation

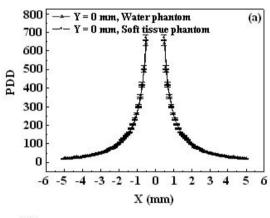
Figure 3 shows the PDD variation along the Y=0 mm, and Y=3 mm for water and soft tissue medium. It is clear that the PDD has been decreased about 10 times in this short distance; as well as the effect of source shield is obvious in this figure. The PDD variation along the X=0.5 mm and X=2 mm are shown in figure 4. It can be seen, due to the low energy photons deposit their energy near the source, the PDD fall down about 7 times when going from X=0.5 mm to X=2 mm, and the PDD curve change from smooth flat shape to a semi-Gaussian shape. The calculated results show a good agreement between water and soft tissue PDD data. The isodose curves for PDD = 100%, 75%, 50% and 25% results in water and soft tissue phantoms are shown at figures 5-a and 5-b. It is well clear that $D = D(r, \theta)$, dose distribution depends to r and θ , distance from the center of source and polar angle, respectively. As seen, the dose is falling in 5 mm from reference point about 4 times. Thus, this seed shouldn't apply in small tumors with size smaller than 5mm.

These results have been used to compute anisotropy function and radial dose function

in next subsection. In our running, the energy cut off was 1eV, the relative error in these calculations is less than 2%, and the time, that is needed for any programs running are about 240 minutes with a computer Pentium 4 Intel CPU 3.06 GHz.

Determination of TG-43 dosimetry parameters

The MCNP calculated results of the anisotropy function, $F(r,\theta)$, against r for the model CS-1 seed at 0° to 80° interval are tabulated in table 3 for water and soft tissue phantoms. Maximum percentage difference of anisotropy function for the phantoms are 2.82%, 3.79%, 4%, 4.71%, 2.31%, 2.53%, 3.49%, 3.80%, 4.67%, 4.72%, 6.17% at r = 0.5, 0.75, 1, 2, 3, 4, 5, 6, and 7 cm, respectively. Most of these maximum differences are to θ=10° angle. The belong demonstrate it would be more exact if dosimetry parameters of soft tissue phantom for medical application used instate of the



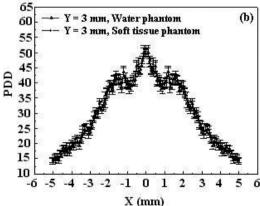


Figure 3. PDD variation along (a) Y= 0 mm and (b) Y=3 mm.

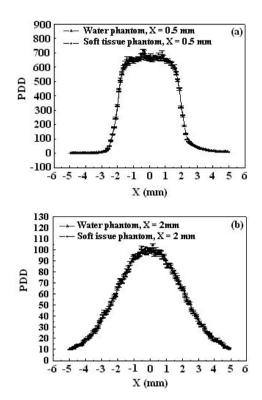


Figure 4. PDD variation along (a) X=0.5 mm and (b) X=2 mm.

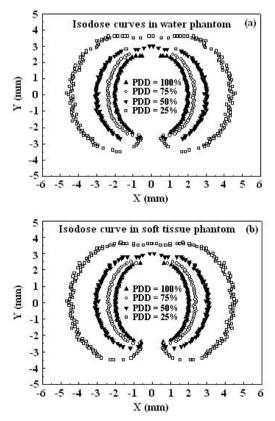


Figure 5. The isodose curves, a) in water phantom, b) in soft tissue phantom (the reference Point: X=2 mm, Y=0 mm).

water data, although near the source data for both phantoms are very close to each other.

DISCUSSION

Radial dose function and anisotropy function are dosimetry important parameters that have been determined to compare our result with which was obtained by others. Our computational results of g(r) against r for the source in water and soft tissue phantoms are shown in figure 6-a. Our results agree well with those of Murphy *et al.* (10) who measured in virtual water phantom. Maximum percentage of difference was about 5.2%. A third order polynomial fit of the MCNP radial dose function in a water medium has been yielded the following relationship:

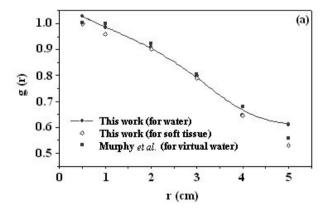
 $g(r) = 0.99465 + 0.01161 r - 0.03696 r^2 + 0.00318 r^3$ The square of correlation coefficient for the polynomial fitting was 0.99778, which was very close to unit as a goodness fitting value.

Also, figure 6-b shows a comparison of F(1 cm, θ) obtained in this study and the results of Murphy *et al.* (10); which maximum difference is 4% at θ =10° and the mean difference was less than 1.5% over the all angels. Therefore, the benchmark of computational results with the experimental results seems compatible.

In conclusion, the isodose curves of the ¹³¹Cs source model CS-1 have been derived form dose calculation for water and soft tissue phantoms by MCNP code. The result shows dose deposition in high gradient region, near the source, can only be calculated accurately by Monte Carlo method. Results show the PDD is falling in about 5 mm from reference point about 4 times. So, this seed dose not advised to apply in small tumors with size smaller than 5mm. calculated TG-43 brachytherapy dosimetry parameters for the source agree quite well with Monte Carlo result of Murphy et al. (10) and are useful in treatment in therapeutic plan. The present demonstrates a useful approach using MCNP code in dose calculation that can be applied in many other fields.

r (cm) θ (deg) 0.75 1 2 3 7 0.5 1.5 2.5 4 5 6 10 0.719 0.729 0.7560.7690.773 0.785 0.796 0.828 0.796 In soft tissue phantom 20 0.792 0.785 0.781 0.808 0.827 0.838 0.847 0.856 0.863 0.864 0.861 30 0.883 0.879 0.854 0.875 0.889 0.891 0.899 0.902 0.895 0.898 0.899 0.927 40 0.922 0.908 0.915 0.922 0.926 0.928 0.939 0.913 0.923 0.931 50 0.9510.952 0.9500.954 0.9580.9590.962 0.969 0.968 0.967 0.968 0.975 60 0.976 0.978 0.977 0.979 0.978 0.979 0.977 0.979 0.975 0.979 70 0.996 0.993 0.993 0.992 0.997 0.988 0.990 0.988 0.987 0.987 0.988 80 1.001 1.003 1.001 0.998 0.997 0.998 0.997 1.003 0.999 0.998 0.997 10 0.7490.7650.7700.7890.801 0.816 0.8350.869 0.836 20 0.821 0.8310.870 0.8720.8860.9010.8150.816 0.812 0.8520.897 30 0.908 0.902 0.903 0.907 0.910 0.912 0.912 0.914 0.917 0.920 0.924 In water phantom 40 0.938 0.939 0.936 0.940 0.944 0.931 0.935 0.941 0.941 0.939 0.937 50 0.966 0.961 0.959 0.961 0.962 0.967 0.969 0.966 0.967 0.970 0.958 60 0.983 0.978 0.9760.977 0.979 0.983 0.981 0.980 0.9820.979 0.97570 0.9910.991 0.9920.989 0.9900.9910.9900.994 0.9880.9890.990

Table 3. Computational value of $F(r, \theta)$ against r at 0° to 80° interval in water and soft tissue phantom.



80

0.998

1.001

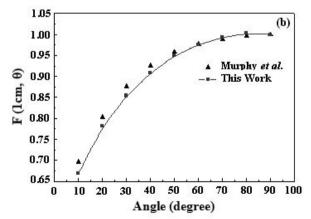
0.996

0.992

1.001

0.998

0.993



0.997

0.994

1.001

0.987

Figure 5. Comparison of the results of this study with the results of Murphy et al. (10) (a) g(r) value against r; (b) F(1 cm, θ) against θ .

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